



Sharif University of Technology
Scientia Iranica
Transactions B: Mechanical Engineering
 www.scientiairanica.com



Developing a finite element beam theory for nanocomposite shape-memory polymers with application to sustained release of drugs

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Received 29 June 2015; received in revised form 19 December 2015; accepted 27 February 2016

KEYWORDS

Shape-memory polymers;
 Finite element;
 Smart beam;
 Euler-Bernoulli beam theory;
 nano/micro reinforcement.

Abstract. In this paper, a thermodynamically consistent constitutive model, recently proposed for nanocomposite Shape-Memory Polymers (SMPs), is used as a basis for development of SMP beam element in a finite element framework. The beam theory utilized here is the Euler-Bernoulli beam theory with its basic assumptions. Effects of different materials as well as the geometric structural parameters, e.g. reinforcement (nano/micro-particles) volume fraction, viscosity coefficients, and external loads, on the thermomechanical response of the structure are studied in this work. The beam element numerical results are compared to those of 3D finite element modeling to verify validity of the beam element formulation and the assumptions made therein. This beam element provides us with a fast and reliable tool for simulation of structures, consisting of reinforced SMP beams. As an application, the developed nanocomposite SMP beam element could be used for numerical modeling of thermomechanical response of the drugs (e.g., theophylline) coated by films of SMP nanocomposites. It is shown that the numerical results are in correspondence with those of the experiments reported for sustained release of SMP-nanocomposite based drugs.

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1. Introduction

Shape-memory materials offer a promising perspective for materials science and engineering, providing access to extensive unconventional functions in various classes of materials: metals, ceramics, and polymers [1]. These materials are capable of returning from a fixed shape to their original shape. This class of materials have been researched, developed, and used in a wide range of applications, such as advanced technologies in the aerospace and medical-related industries [2–5]. The Shape-Memory Effect (SME) is normally in-

duced through external stimuli, e.g. heat, electricity, or magnetism [6,7]. The mechanisms controlling the thermally activated SME in Shape-Memory Polymers (SMPs) are different from those that play roles in shape-memory alloys or ceramics. These phenomena result in differences in the thermomechanical responses of the material [8].

However, the much smaller stiffness of un-reinforced SMPs limits their practical applications, in which a larger recovery stress is necessary. To get over such limitations, different reinforcement techniques are introduced in the literature [9–13]. The necessity to activate SMPs through non-thermal stimuli has led to employing conductive fillers, e.g. conductive particles, nanocarbon particles, and conductive fibers [14–17]. The SMP composites are considered as a conductive

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polymer with potential practical applications in the fields of micro-sensors and actuators. Thus, different chemical sensors and bio-sensors with fascinating characteristics could be designed and used in medicine for fast bio-diagnostic systems [15,18–20].

It should be noted that multifunctional polymers combining two functions, such as SME and biodegradability [21] or biodegradability and drug release [22], have already been introduced [23]. But, a material that exhibits all these three functions has not been deeply investigated yet. This would let us use SME to perform minimally invasive implantation of quite massive devices, biodegradability to eliminate a second surgery for removal, and controlled drug release during encountering infections [24]. In a very recent study, Kashif et al. [25] investigated the sustained drug release and hydrolytic degradation of biodegradable shape-memory poly(ϵ -caprolactone)/polyhedral oligomeric silsesquioxane nanocomposites. In vitro drug release, investigations of the phosphate buffer solution (pH = 7.4) showed that TspPOSS nanocomposite nanocrystals led to sustained release of the drug for the nanocomposites. PCL/TspPOSS nanocomposite (90 wt/10 wt) containing 10 wt% drug (Theophylline) demonstrated good thermally activated SME with a shape fixation ratio of 81% and shape recovery ratio of 85%.

Some researchers also investigated the effect of addition of nano-particles into SMP matrix [26,27]. Zhang and Ni [28] performed some experiments to study the effects of carbon fiber fabric reinforcement on the mechanical behavior of SMP sheets. The resulting SMP based laminates possessed good shape recoverability. They also showed that the bending recovery ratio was high compared to that of the SMP sheet at different recovery durations [28]. Despite a variety of SMP applications involving bending loads, bending characterizations are not much extensive [29,30]. Some researchers tried to experimentally characterize the behavior of SMPs [11,30–33]. Up to now, characterization of the SMP behavior has been carried out with uniaxial tests [11,31–34]; however, flexural thermomechanical tests could aid the characterization of an SMP constitutive model.

Proposing an elastic-predictor inelastic-corrector, Ghosh et al. [5] introduced a finite element SMP beam based on a constitutive model already published by the same authors. Baghani et al. [35] presented analytic expressions for deflection of an SMP beam utilizing Euler-Bernoulli beam theory in a thermomechanical SME cycle. They employed the constitutive model already proposed in [36], where time-dependent effects were neglected. In another work, Baghani and Taheri [37] extended this method to investigate the mechanical behavior of reinforced SMP beams.

In this paper, we propose finite element solutions for nanocomposite SMP beams in an arbitrary loading-displacement recovery cycle. Employing the Euler-Bernoulli beam theory, a 1D SMP beam element is proposed. This formulation is helpful in simulation of structures that consist of SMP beams. This newly introduced SMP beam element can be utilized for either parametric study (material or geometrical parameters) of the SMP beam behavior or design and optimization involving a large number of simulations in which computational cost is a critical parameter. Making use of this beam element dramatically decreases the computational cost, compared to 3D general element previously proposed by Baghani et al. [38]. We also investigate the SME of SMP nanocomposites to qualitatively study its drug release characteristics.

The paper is organized as follows. Firstly, a 3D constitutive equation for SMPs is briefly reviewed in Section 2. Then, in Section 3, the 3D constitutive relations are reduced to the cases in which Euler-Bernoulli beams undergo arbitrary bending loadings. In this section, development of the SMP beam finite element is discussed in detail. In Section 4, by employing the newly introduced SMP beam element, some numerical examples are solved. It will be shown that the numerical results are in correspondence with those of experiments reported for sustained release of SMP-nanocomposite based drugs. Results of the present work are compared to those of 3D modeling already published by the same authors as well as some experiments available in the literature. Finally, in Section 5, we present a summary and draw conclusions.

2. Brief review of the SMP constitutive model development

Since the shape-memory effect characteristics are discussed in details in some already published papers by the same authors, in this paper, for the sake of brevity, we avoid repeating these details and refer to [36,38–40]. In those papers, the 3D diagrams of stress-strain-temperature for both *stress-free strain recovery* and *fixed-strain stress recovery* are introduced.

Baghani et al. [36] proposed a constitutive model for SMPs in the small strain regime. They then extended this model to time-dependent loading conditions in [38]; in this work, we employ this model to properly account for thermomechanical response of SMPs. They also extended this model to the domain of large strains employing two different approaches [40,41]. As described in [36,38–40], it has been assumed that the rubbery and glassy phases are able to be transformed into each other, through the external stimuli of heat. The evolution laws for internal variables have been derived in an arbitrary thermomechanical loading. They have decomposed the

strain into four parts as:

$$\boldsymbol{\varepsilon} = \phi_p \boldsymbol{\varepsilon}^p + \phi_h \boldsymbol{\varepsilon}^h + \boldsymbol{\varepsilon}^i + \boldsymbol{\varepsilon}^T, \quad (1)$$

where superscripts p and h stand for the SMP and hard segments, respectively. Also, $\boldsymbol{\varepsilon}^i$ and $\boldsymbol{\varepsilon}^T$ are the irreversible and thermal strains, respectively, while $\boldsymbol{\varepsilon}^p$ is the strain in SMP segment. ϕ_p and ϕ_h denote the volume fractions of the SMP and hard segments, respectively ($\phi_p + \phi_h = 1$). Besides, the strain in the SMP segment is decomposed into three parts as:

$$\boldsymbol{\varepsilon}^p = \varphi_r \boldsymbol{\varepsilon}^r + \varphi_g \boldsymbol{\varepsilon}^g + \boldsymbol{\varepsilon}^{is}, \quad (2)$$

where subscripts r and g stand for the rubbery and glassy phases, respectively. Also, φ_r and φ_g are volume fractions of the rubbery and glassy phases, respectively ($\varphi_r + \varphi_g = 1$). It is noted that φ_r and φ_g are temperature-dependent functions, while ϕ_p and ϕ_h are constant parameters. $\boldsymbol{\varepsilon}^{is}$ is the stored strain in the material and evolves in the following form [38]:

$$\dot{\boldsymbol{\varepsilon}}^{is} = \dot{\varphi}_g \left(k_1 \boldsymbol{\varepsilon}^r + k_2 \frac{\boldsymbol{\varepsilon}^{is}}{\varphi_g} \right),$$

where:

$$\begin{cases} k_1 = 1, & k_2 = 0; & \dot{T} < 0 \\ k_1 = 0, & k_2 = 1; & \dot{T} > 0 \\ k_1 = 0, & k_2 = 0; & \dot{T} = 0 \end{cases} \quad (3)$$

where dot denotes differentiation with respect to time. Moreover, to account for the viscoelastic behavior of SMPs, some other decompositions are assumed. In the range of small strains, strains are additively decomposed in the glassy, rubbery, and hard phases as:

$$\boldsymbol{\varepsilon}^r = \boldsymbol{\varepsilon}^{er} + \boldsymbol{\varepsilon}^{ir}, \quad \boldsymbol{\varepsilon}^g = \boldsymbol{\varepsilon}^{eg} + \boldsymbol{\varepsilon}^{ig}, \quad \boldsymbol{\varepsilon}^h = \boldsymbol{\varepsilon}^{eh} + \boldsymbol{\varepsilon}^{ih}, \quad (4)$$

in which the superscripts $e\beta$ and $i\beta$ ($\beta = r, g, h$) denote the elastic and inelastic (viscous) parts of the strain in all phases, respectively. Employing the mixture rule, the free-energy density function, Ψ , for an amorphous reinforced SMP is introduced as:

$$\begin{aligned} \Psi(\boldsymbol{\varepsilon}, T, \phi_p, \phi_h, \varphi_g, \boldsymbol{\varepsilon}^r, \boldsymbol{\varepsilon}^{er}, \boldsymbol{\varepsilon}^g, \boldsymbol{\varepsilon}^{eg}, \boldsymbol{\varepsilon}^h, \boldsymbol{\varepsilon}^{eh}) \\ = \phi_h \Psi_h(\boldsymbol{\varepsilon}^h, \boldsymbol{\varepsilon}^{eh}) + \Psi_T(T) \\ + \phi_p [\varphi_r \Psi_r(\boldsymbol{\varepsilon}^r, \boldsymbol{\varepsilon}^{er}) + \varphi_g \Psi_g(\boldsymbol{\varepsilon}^g, \boldsymbol{\varepsilon}^{eg})] \\ + \Psi_\lambda(\boldsymbol{\varepsilon}, T, \phi_p, \phi_h, \varphi_r, \varphi_g, \boldsymbol{\varepsilon}^r, \boldsymbol{\varepsilon}^g, \boldsymbol{\varepsilon}^{is}, \boldsymbol{\varepsilon}^h, \boldsymbol{\varepsilon}^i), \end{aligned} \quad (5)$$

in which Ψ_r , Ψ_g , and Ψ_h are Helmholtz free-energy density functions of the rubbery, glassy, and hard phases, respectively. Temperature is denoted by T and the thermal energy is represented by Ψ_T . Besides, to

satisfy Eqs. (1), (2), and (4) in the formulation, using the method of Lagrange multipliers, the term Ψ_λ is added into the free energy as:

$$\begin{aligned} \Psi_\lambda(\boldsymbol{\varepsilon}, T, \phi_p, \phi_h, \varphi_r, \varphi_g, \boldsymbol{\varepsilon}^r, \boldsymbol{\varepsilon}^g, \boldsymbol{\varepsilon}^{is}, \boldsymbol{\varepsilon}^h, \boldsymbol{\varepsilon}^i) \\ = \boldsymbol{\lambda} : [\boldsymbol{\varepsilon} - \phi_p(\varphi_r \boldsymbol{\varepsilon}^r + \varphi_g \boldsymbol{\varepsilon}^g + \boldsymbol{\varepsilon}^{is}) - \phi_h \boldsymbol{\varepsilon}^h - \boldsymbol{\varepsilon}^i - \boldsymbol{\varepsilon}^T], \end{aligned} \quad (6)$$

in which $\boldsymbol{\lambda}$ is the Lagrange multiplier. They also defined:

$$\begin{aligned} \Psi_\beta(\boldsymbol{\varepsilon}^\beta, \boldsymbol{\varepsilon}^{e\beta}) = \Psi_\beta^{eq}(\boldsymbol{\varepsilon}^\beta) + \Psi_\beta^{neq}(\boldsymbol{\varepsilon}^{e\beta}), \\ \beta = r, g, h, \end{aligned} \quad (7)$$

in which the superscripts ‘eq’ and ‘neq’ are the equilibrium and non-equilibrium parts of $\Psi_\beta(\boldsymbol{\varepsilon}^\beta, \boldsymbol{\varepsilon}^{e\beta})$. In this model, it is emphasized that the internal variables are φ_g , $\boldsymbol{\varepsilon}^{ir}$, $\boldsymbol{\varepsilon}^{ig}$, $\boldsymbol{\varepsilon}^{ih}$, $\boldsymbol{\varepsilon}^i$, and $\boldsymbol{\varepsilon}^{is}$. Thus, evolution laws for the internal variables in the context of continuum thermodynamics should be introduced.

Satisfying the second law of thermodynamics in the form of Clausius-Duhem inequality gives:

$$\begin{aligned} \boldsymbol{\sigma} &= \frac{\partial \Psi_r^{eq}}{\partial \boldsymbol{\varepsilon}^r} + \frac{\partial \Psi_r^{neq}}{\partial \boldsymbol{\varepsilon}^{er}} = \frac{\partial \Psi_g^{eq}}{\partial \boldsymbol{\varepsilon}^g} + \frac{\partial \Psi_g^{neq}}{\partial \boldsymbol{\varepsilon}^{eg}} \\ &= \frac{\partial \Psi_h^{eq}}{\partial \boldsymbol{\varepsilon}^h} + \frac{\partial \Psi_h^{neq}}{\partial \boldsymbol{\varepsilon}^{eh}}. \end{aligned} \quad (8)$$

Furthermore, in accordance with the viscoelastic behavior of polymers, the following evolution laws are sufficient conditions for satisfaction of Clausius-Duhem inequality [38]:

$$\begin{aligned} \dot{\boldsymbol{\varepsilon}}^{ir} &= \frac{1}{\eta_r} \frac{\partial \Psi_r^{neq}}{\partial \boldsymbol{\varepsilon}^{er}}, & \dot{\boldsymbol{\varepsilon}}^{ig} &= \frac{1}{\eta_g} \frac{\partial \Psi_g^{neq}}{\partial \boldsymbol{\varepsilon}^{eg}}, \\ \dot{\boldsymbol{\varepsilon}}^{ih} &= \frac{1}{\eta_h} \frac{\partial \Psi_h^{neq}}{\partial \boldsymbol{\varepsilon}^{eh}}, & \dot{\boldsymbol{\varepsilon}}^i &= \frac{1}{\eta_i} \boldsymbol{\sigma}, \end{aligned} \quad (9)$$

in which η_r , η_g , η_h , and η_i are viscosity coefficients of the rubbery, glassy, hard, and irreversible parts, respectively.

3. Development of an SMP Euler-Bernoulli beam element

In this section, it is assumed that equilibrium and nonequilibrium elastic strain energies are in the forms of $\Psi_\beta^{eq}(\boldsymbol{\varepsilon}^\beta) = \frac{1}{2} \boldsymbol{\varepsilon}^\beta : \mathbb{K}_\beta^{eq} : \boldsymbol{\varepsilon}^\beta$ and $\Psi_\beta^{neq}(\boldsymbol{\varepsilon}^{e\beta}) = \frac{1}{2} \boldsymbol{\varepsilon}^{e\beta} : \mathbb{K}_\beta^{neq} : \boldsymbol{\varepsilon}^{e\beta}$, $\beta = r, g, h$, in which \mathbb{K}_β^{eq} 's and \mathbb{K}_β^{neq} 's are fourth-order elasticity tensors corresponding to each phase.

Following the general procedure presented by Reddy [42], we employ the basic assumptions of Euler-Bernoulli beam theory, in which the bending of beams

with small strains and rotations is found from the following displacement field:

$$u_1 = -z \frac{dw}{dx}, \quad u_2 = 0, \quad u_3 = w(x), \quad (10)$$

where u_1 , u_2 , and u_3 are the displacements of a material point at the location (x, y, z) . u and w are the axial and transverse displacements of the geometric centroid of the cross section on the x -axis. An additional assumption has also been made: Transverse loads only cause transverse displacement and no shear strain is generated. Thus, the following linear strain is obtained:

$$\varepsilon_{xx} = -z \frac{d^2 w}{dx^2}. \quad (11)$$

Since we aim to develop Euler-Bernoulli beam element for SMPs, the constitutive model presented in Section 2 should be reduced to the case where only axial strain (along beam axis) exists. Moreover, we should present the time-discrete form of the SMP constitutive model. We subdivide the time interval of interest $[0, t]$ in sub-increments and solve the nonlinear problem over the generic interval $[t_n, t_{n+1}]$ with $t_{n+1} > t_n$. For the sake of simplicity, we indicate with the subscript n a quantity evaluated at time t_n and with no subscript a quantity evaluated at time t_{n+1} . We also show the time increment by Δt . Knowing the solution and the strain ε_n at time t_n , as well as the strain ε at time t_{n+1} , the stress and the internal variables should be updated from the deformation history. Therefore, the time-discrete implicit form of the SMP constitutive model, specifically in Eq. (3), yields:

$$\begin{aligned} \varepsilon^{is} &= \varepsilon_n^{is} + k_1 \Delta \varphi \varepsilon^r + k_2 \varphi^{-1} \Delta \varphi \varepsilon^{is} \\ \Rightarrow \varepsilon^{is} (1 - k_2 \varphi^{-1} \Delta \varphi) &= \varepsilon_n^{is} + k_1 \Delta \varphi \varepsilon^r. \end{aligned} \quad (12)$$

Moreover, discretizing Eq. (9) and recasting Eq. (12) give:

$$\begin{cases} \varepsilon^{i\beta} = c_\beta^{-1} (\sigma + E_\beta b_\beta \varepsilon_n^{i\beta}); & \beta = r, g, h \\ \varepsilon^i = \varepsilon_n^i + b_i \sigma \\ \varepsilon^{is} = k_3^{-1} (\varepsilon_n^{is} + k_4 ((b_r + 1) \varepsilon^{ir} - b_r \varepsilon_n^{ir})) \end{cases}$$

where:

$$\begin{cases} k_3 = 1 - k_2 \varphi^{-1} \Delta \varphi \\ k_4 = k_1 \Delta \varphi \end{cases} \quad (13)$$

$$\begin{aligned} b_\beta &= \frac{\eta_\beta}{\Delta t E_\beta^{\text{neq}}}, & b_i &= \frac{\Delta t}{\eta_i}, & c_\beta &= E_\beta b_\beta + E_\beta^{\text{eq}}, \\ E_\beta &= E_\beta^{\text{eq}} + E_\beta^{\text{neq}}, & \beta &= r, g, h. \end{aligned} \quad (14)$$

Eqs. (12) to (14) show how internal variables are updated in Δt . Furthermore, after some mathematical manipulations, the axial stress is updated by Eq. (15) as shown in Box I. Eq. (15) can be recast as:

$$\sigma = \chi_1 \varepsilon^m + \chi_2, \quad (16)$$

in which parameters χ_1 and χ_2 are defined by Eq. (17) as shown in Box II. Eq. (16) in terms of the transverse deflection yields:

$$\begin{aligned} \sigma &= \chi_1 \varepsilon^m + \chi_2 = \chi_1 (-y w'') + \chi_2 y \\ &= y (-\chi_1 w'' + \chi_2), \end{aligned} \quad (18)$$

where prime stands for differentiation with respect to x . As observed in Eq. (18), the stress varies linearly within the beam height. Computing the moment about the z -axis, we may write:

$$\begin{aligned} M &= - \int_A \sigma y dA = - \int_A (-\chi_1 w'' + \chi_2 y) y^2 dA \\ &= (\chi_1 w'' - \chi_2 y) I, \end{aligned} \quad (19)$$

in which I and M denote the moment of inertia and the moment along z -axis, respectively. A also stands for cross sectional area of the beam. We now recast Eq. (19) as:

$$\begin{aligned} M &= \psi_1 w'' + \psi_2, \\ \text{where:} \\ \psi_1 &= \chi_1 I, & \psi_2 &= -\chi_2 y I. \end{aligned} \quad (20)$$

$$\sigma = \frac{\left[\left(\varepsilon_n^{is} + k_3 (b_h \varepsilon_n^{ih} - b_g \varepsilon_n^{ig} \varphi) + b_r \varepsilon_n^{ir} (k_3 (\varphi - 1) - k_4) \right) \phi_p + (\varepsilon_n^i - b_h \varepsilon_n^{ih} - \varepsilon^m) k_3 \right) c_r c_g c_h + (c_h (b_g + 1) b_g \varepsilon_n^{ig} E_g \phi_p \varphi + (1 - \phi_p) (b_h + 1) b_h \varepsilon_n^{ih} E_h c_g) c_r k_3 + (k_3 + k_4 - k_3 \varphi) (b_r + 1) b_r \phi_p \varepsilon_n^{ir} E_r c_g c_h \right]}{((1 + b_g) \phi_p \varphi + a_4 c_g) c_h + (b_h + 1) (1 - \phi_p) c_g) k_3 c_r + (k_3 (1 - \varphi) + k_4) (b_r + 1) \phi_p c_g c_h} \quad (15)$$

where ε^m denotes the mechanical part of the total strain ($\varepsilon^m = \varepsilon - \varepsilon^T$).

$$\begin{cases} \chi_1 = \frac{c_r c_g c_h k_3}{\chi_3} \\ \chi_2 = \frac{-1}{\chi_3} \left(\left(\begin{bmatrix} \varepsilon_n^{is} + k_3(b_h \varepsilon_n^{ih} - b_g \varepsilon_n^{ig} \varphi) \\ + b_r \varepsilon_n^{ir} (k_3(\varphi - 1) - k_4) \end{bmatrix} \phi_p + (\varepsilon_n^i - b_h \varepsilon_n^{ih}) k_3 \right) c_r c_g c_h \right. \\ \left. + (c_h(b_g + 1) b_g \varepsilon_n^{ig} E_g \phi_p \varphi + (1 - \phi_p)(b_h + 1) b_h \varepsilon_n^{ih} E_h c_g) c_r k_3 \right. \\ \left. + (k_3 + k_4 - k_3 \varphi)(b_r + 1) b_r \phi_p \varepsilon_n^{ir} E_r c_g c_h \right) = \chi_{2y} y \\ \chi_3 = (((1 + b_g) \phi_p \varphi + a_4 c_g) c_h + (b_h + 1)(1 - \phi_p) c_g) k_3 c_r + (k_3(1 - \varphi) + k_4)(b_r + 1) \phi_p c_g c_h \end{cases} \quad (17)$$

Box II

The weak form is the result of the principle of virtual displacements. It states that if a body is in equilibrium, the total virtual work done by actual internal and external forces in moving through the virtual displacements is zero. This principle over a finite element $x \in [0, l^e]$, is:

$$\delta W^e = \delta W^E + \delta W^I = 0, \quad (21)$$

where δW^I is the internal virtual work, and δW^E is the external work done by the externally applied loads through the virtual displacements. The schematics of the beam element with the defined relevant degrees of freedom are shown in Figure 1.

The virtual work principle for the Euler-Bernoulli beam theory is reduced to:

$$\delta W^e = \int_A \int_0^{l^e} \sigma \delta \varepsilon dx dA - \int_0^{l^e} q(x) \delta w dx - \sum_{i=1}^4 Q_i \delta \Omega_i, \quad (22)$$

where l^e is length of the element, $q(x)$ is the distributed transverse loads measured per unit length, Q_i 's are the generalized nodal forces, and $\delta \Omega_i$ are the virtual generalized nodal displacements of the element. Thus, in light of definition (11), the virtual work statement in Eq. (21) becomes:

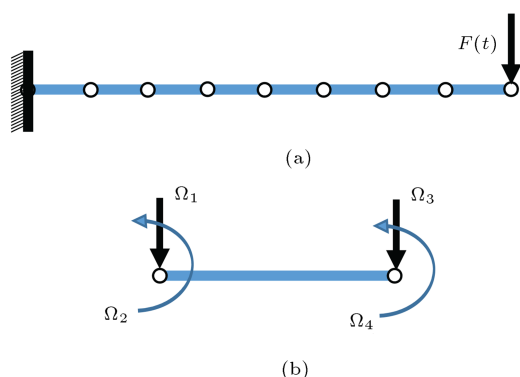


Figure 1. The schematics of the beam element together with the defined degrees of freedom.

$$\begin{aligned} \delta \varepsilon &= -y \frac{d^2(\delta w)}{dx^2} \\ \Rightarrow \int_A \int_0^{l^e} \sigma \delta \varepsilon dx dA &= - \int_0^{l^e} \frac{d^2(\delta w)}{dx^2} \overbrace{\int_A \sigma y dA}^{-M(x)} dx. \end{aligned} \quad (23)$$

Substituting Eq. (23) into Eq. (22) yields:

$$\begin{aligned} \delta W^e &= \int_0^{l^e} \frac{d^2(\delta w)}{dx^2} M(x) dx - \int_0^{l^e} q(x) \delta w dx \\ &\quad - \sum_{i=1}^4 Q_i \delta \Omega_i = 0. \end{aligned} \quad (24)$$

In light of Eqs. (20) and (24), we arrive at:

$$\begin{aligned} \int_0^{l^e} \frac{d^2(\delta w)}{dx^2} \left[\psi_1 \frac{d^2 w}{dx^2} + \psi_2 \right] dx - \int_0^{l^e} q(x) \delta w dx \\ - \sum_{i=1}^4 Q_i \delta \Omega_i = 0. \end{aligned} \quad (25)$$

Employing 1D Hermite cubic interpolation function N_i , the transverse beam deflection is approximated in terms of four degrees of freedom, i.e. Ω_i , as:

$$w = \sum_{i=1}^4 N_i \Omega_i, \quad \delta w = \sum_{i=1}^4 N_i \delta \Omega_i, \quad (26)$$

where these degrees of freedom are:

$$\begin{aligned} \Omega_1 &= w(0), & \Omega_2 &= -dw/dx|_{x=0}, \\ \Omega_3 &= w(l^e), & \Omega_4 &= -dw/dx|_{x=l^e}. \end{aligned} \quad (27)$$

Substituting Eq. (26) into Eq. (25), after some mathematical manipulations, gives:

$$\sum_{i=1}^4 \left(\int_0^{l^e} \frac{d^2 N_i}{dx^2} \left[\psi_1 \frac{d^2 w}{dx^2} + \psi_2 \right] dx - \int_0^{l^e} N_i q(x) dx - Q_i \right) \delta \Omega_i = 0. \quad (28)$$

Assuming w in the form of Eq. (26), Eq. (28) is rewritten as follows:

$$\int_0^{l^e} \frac{d^2 N_i}{dx^2} \left[\psi_1 \sum_{j=1}^4 \frac{d^2 N_j}{dx^2} \Omega_j + \psi_2 \right] dx - \int_0^{l^e} q(x) N_i dx - Q_i = 0. \quad (29)$$

In order to present the matrix format for the element stiffness and load vectors, Eq. (29) is finally recast as:

$$[K_{ij}] \{\Omega_j\} = \{F_i\}, \quad (30)$$

in which:

$$\begin{cases} K_{ij} = \psi_1 \int_0^{l^e} \frac{d^2 N_i}{dx^2} \frac{d^2 N_j}{dx^2} dx \\ F_i = -\psi_2 \int_0^{l^e} \frac{d^2 N_i}{dx^2} dx + \int_0^{l^e} q(x) N_i dx + Q_i \end{cases} \quad (31)$$

For the sake of completeness, the Hermite shape functions are reported as follows:

$$\begin{aligned} N_1 &= \frac{2x^3 - 3x^2 l^e + l^{e^3}}{l^{e^3}}, & N_2 &= \frac{x^3 l^e - 2x^2 l^{e^2} + x l^{e^3}}{l^{e^3}}, \\ N_3 &= \frac{-2x^3 + 3x^2 l^e}{l^{e^3}}, & N_4 &= \frac{x^3 l^e - x^2 l^{e^2}}{l^{e^3}}. \end{aligned} \quad (32)$$

It is finally reminded that ψ_1 and ψ_2 are memory parameters. These parameters are updated in each increment and are responsible for the history dependency of the SMP element response, as described in Eqs. (17) and (20).

4. Numerical results

To show validity of the model in time-dependent regimes of thermomechanical loadings, we first report the simulation results according to experiments performed in [43] already published in [38]. At the start of the experiment, an SMP-based syntactic foam sample is compressed under a constant stress $\sigma_0 = -263$ kPa at T_h for 30 minutes. Keeping the stress fixed, the temperature is lowered to T_l . The cooling rate is found through the Newton's law of cooling: $\frac{dT}{dt} = 4.6 \times 10^{-5} (T - 293)$ [38]. Once the temperature reaches T_l (at $t = 1256$ min), the system is unloaded and, then, it is heated up to T_h with heating rate $= 0.3 \frac{\text{K}}{\text{min}}$. The required material parameters are tabulated in Table 1. The strain-time behavior is shown in Figure 2(a). A good correlation is observed between the experiments and the numerical results. If the recovery occurs in a *fixed-strain stress recovery*, the stress-temperature behavior is found as shown in

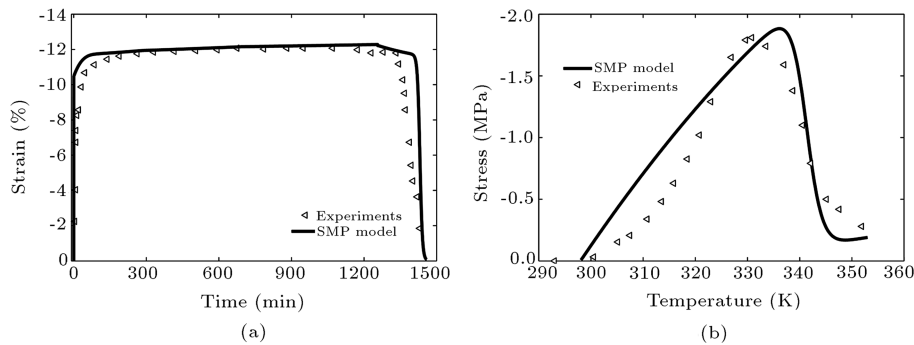


Figure 2. Reproduction of the shape-memory effect [38]: (a) *Stress-free strain recovery* and (b) *fixed-strain stress recovery*. Experiments are reported in [43].

Table 1. Material parameters reported by Baghani et al. [38] adopted from experiments conducted in [43].

Material parameters	Values	Units
$E_r^{\text{eq}}, E_g^{\text{eq}}, E_h^{\text{eq}}, E_r^{\text{neq}}, E_g^{\text{neq}}, E_h^{\text{neq}}$	1.3, 15,70000, 0.2, 247,1000	(MPa)
η_r, η_g, η_h	$5, 30 \times 10^6, 30 \times 10^9$	(MPa.min)
ν_r, ν_g, ν_h	0.49, 0.3, 0.3	(-)
T_l, T_g, T_h	296, 344, 353	(K)
ε^T	$(0.5542 \times 10^{-3} T - 0.01083 - 7 \times 10^{-7} T^2)$	(-)
φ_g	$1 - \frac{1}{1 + \exp(-0.66(T - T_g))}$	(-)

Figure 2(b). These results show that the SMP model is capable of predicting the main governing phenomena in different SME cycles.

Now, we employ the presented SMP beam element to investigate the bending of a cantilever SMP beam, experiencing a *stress-free strain recovery* cycle. An I-shaped SMP beam is selected for presenting the numerical results. Thickness of the beam cross section is 1 mm and its height and width are 10 mm and 12 mm, respectively. The history of the applied force on the free tip of the beam, as well as the temperature history, is shown in Figure 3. Making

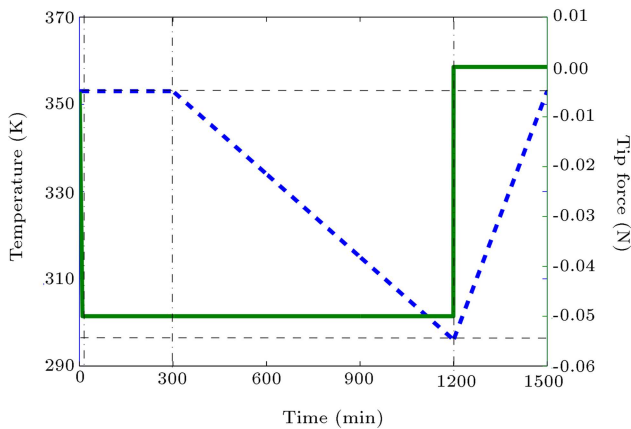


Figure 3. History of the force and temperature applied to the beam.

use of the material parameters reported in Table 1, the corresponding results are illustrated in Figure 4. In order to validate results of the present work, the 3D SMP constitutive model is implemented in a finite element framework. For 3D simulations, we use the nonlinear finite element software ABAQUS/Standard, implementing the described algorithm in [38] within a user-defined subroutine UMAT. Employing this 3D finite element tool, the whole SME cycle is simulated. In Figure 4(a), the free tip displacement results of the SMP beam model (present work) together with those of the 3D modeling are depicted. As one may observe, at different values of ϕ_h , an acceptable correspondence is seen between the results of these two methods. Moreover, at larger values of ϕ_h , as expected, the structure becomes stiffer. Hence, smaller beam tip deflections are predicted. Besides, as observed in Figure 4(a), the beam is capable of complete recovery of the shape. It can be justified considering that in this example, η_i has a very large value. As a result, no residual irreversible strain remains in the structure. The time-dependent viscoelastic behavior of the structure at temperatures higher than T_h is clearly seen in Figure 4(a).

In Figure 4(b), the variations of axial strain at upper surface of the beam root (the most critical point of the structure) are plotted. This figure shows that the maximum strain is about 3.3%. Thus, the small

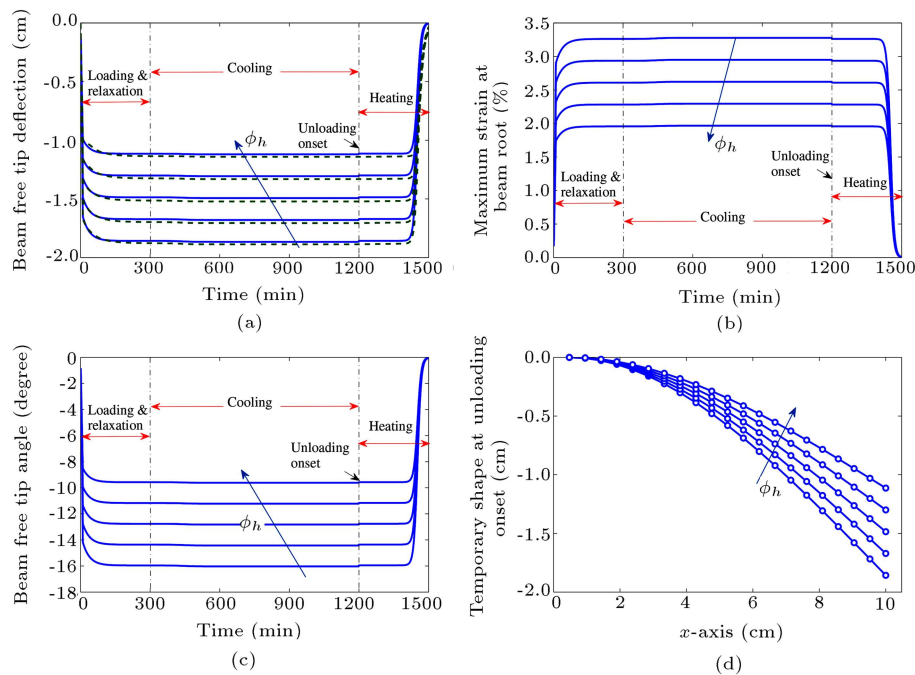


Figure 4. Effect of ϕ_h on (a) the free tip displacement results of the SMP beam model (present work) together with those of the 3D modeling (solid lines show the beam element results, while dashed-lines represent the 3D finite element predictions), (b) variation of axial strain at upper surface of the beam root (the most critical point of the structure), (c) the free tip angle of the beam, and (d) the temporarily memorized shape of the beam (after unloading). $F_{\max} = -0.05$ N, $q = 0$ (N/m), and $\phi_h = 0, 0.1, 0.2, 0.3, 0.4$.

strain assumption used in developing the element is not violated. Moreover, in Figure 4(c), the free tip angle of the beam is shown. This figure also shows the maximum angle smaller than 16 degrees. Thus, the assumption of small rotations also stands. In Figure 4(d), the temporary shape of the beam (after unloading) is depicted at different ϕ_h 's.

In order to investigate the effects of different values of viscosity parameters, in Figure 5, the free tip displacement results of the SMP beam model are depicted. It is shown that increasing η_r makes the structure need more time to react against the applied stress. To investigate the effect of applying an external force during the heating process on the shape recovery, free tip of the beam is plotted in Figure 6. In this figure, F_{\max} is the maximum force applied to free tip of the beam in the loading path and F_h is the force applied to the beam within the heating process. As observed in Figure 6, without any external force ($F_h = 0$), the SMP beam fully recovers its original shape, while increasing the external force (during the heating) results in smaller values of recovery ratio as illustrated in Figure 6. In the special case where $F_h = F_{\max}$, we almost have no recovery. It shows that after heating recovery, stored strains completely vanish and responses of the structure to the mechanical loadings are similar to the first responses, i.e. those at T_h .

The developed formulation can be used in any

Table 2. SMP behavior of theophylline-loaded PCL/TspPOSS (90/10) nanocomposites [25].

Theophylline weight (%)	Shape fixity (%)	Shape recovery (%)
0	85	94
5	82	87
10	81	74

structure that undergoes bending. If we want to properly model a drug in which an SMP-nanocomposite is coated on the drug, e.g. theophylline, we should just use the SMP beam element developed here, accompanied by elastic/hyperelastic/viscoelastic elements (these elements stand for the drug, e.g. theophylline parts). In Table 2, the recovery and shape fixity ratios of the SMP-nanocomposite drug are tabulated. These data are borrowed from [25]. As one may observe in this table, increasing the weight fraction of theophylline leads to a decrease in the shape recovery as well as the shape fixity of the drug. This trend is qualitatively in agreement with those found in this paper.

5. Summary and conclusions

In this work, by employing a new constitutive model recently proposed for SMPs, a new SMP beam element was developed in a finite element framework to predict the response of reinforced SMP beams under

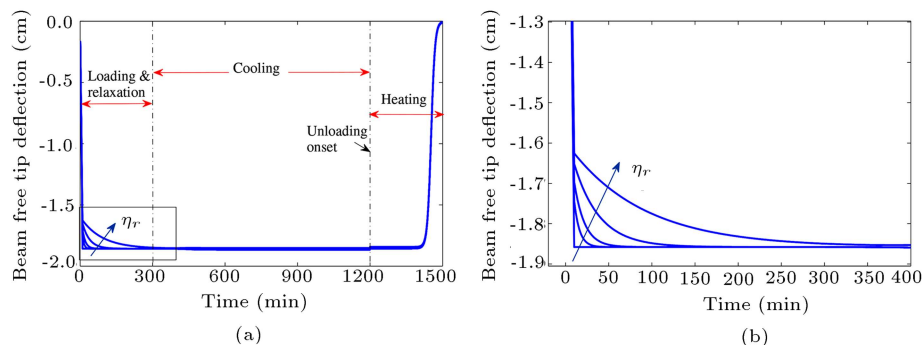


Figure 5. (a) Effect of η_r on the free tip displacement results of the SMP beam model ($\eta_r = 0, 1, 2, 5, 10$ MPa.min and $\phi_h = 0$). (b) The rectangle in part (a) is zoomed in.

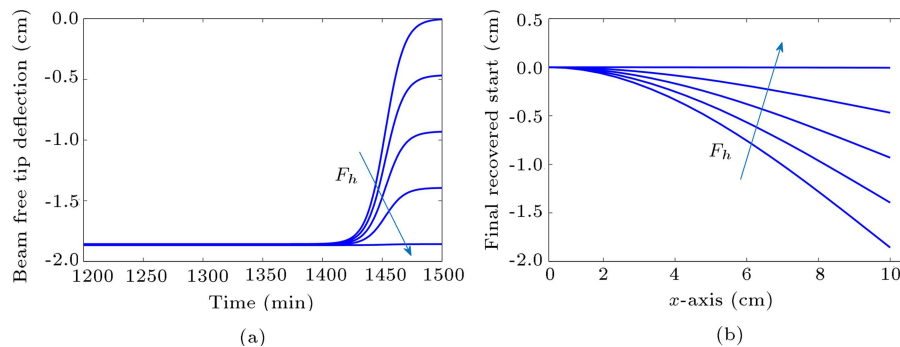


Figure 6. Effect of applying an external force during the heating process to the shape recovery on (a) the free tip displacement and (b) the recovered shape ($F_h/F_{\max} = 0.0, 0.1, 0.2, 0.5, 1.0$ and $\phi_h = 0$).

bending in thermo-mechanical cycles. To develop the formulations, the assumptions of Euler-Bernoulli beam theory were employed. It was observed that within the cooling (shape fixation) process, the stored strains evolved to fix the temporary shape; then, during the heating process, these strains started to relax, in order to recover the original shape. Effects of different values of hard segment volume fraction on the SMP beam response for a cantilever reinforced SMP beam were also investigated. It was observed that increasing volume fraction of hard segment acted as reinforcement and made the structure stiffer. Thus, as a conclusion, larger values of external loads could be handled. Moreover, the time-dependent effects were investigated through a parametric study on the viscosity coefficient in the rubbery phase. It was shown that in larger values of η_r , the structure needed more time to arrive at a steady state. With no external forces within the heating step, the SMP beam almost fully recovered its original shape, while increasing the external force (during heating) resulted in smaller values of recovery ratio. In the special case that the external loadings were same as the loadings in the loading step, the structure experienced almost no shape recovery. Comparing the numerical results with those of 3D finite element modeling ensures the validity of the beam element developments and the assumptions made therein. The proposed finite element beam formulation can be used as an efficient tool for investigating the effects of changing any material or geometrical parameter on reinforced SMP beams, where we need a large number of simulations and 3D modeling is computationally too expensive. As an application, it was shown that the developed nanocomposite SMP beam element could be used for numerical modeling of thermomechanical response of the drugs (e.g., theophylline) coated by films of SMP nanocomposites. It was observed that the numerical results were qualitatively in correspondence with those of experiments reported for sustained release of SMP-nanocomposite based drugs already available in the literature.

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